

Biomedical Image Analysis



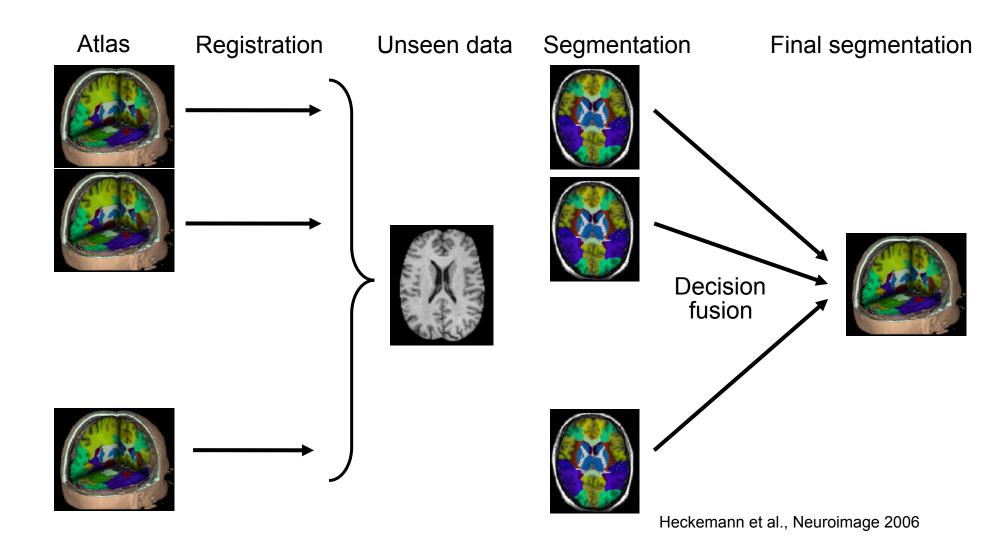
Manifold Learning: Applications in Neuroimaging

Robin Wolz 23/09/2011

Overview

- Manifold learning for Atlas Propagation
 - Multi-atlas segmentation
 - Challenges
 - LEAP
- Manifold learning for classification
 - Cross-sectional data
 - Longitudinal data
 - Metadata
- Conclusions

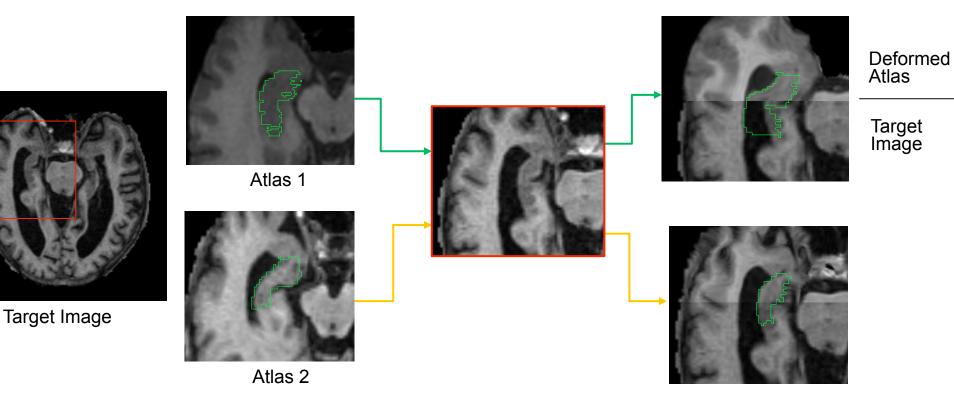
Segmentation using multi-atlas fusion



Segmentation using multi-atlas fusion

Problems:

- Number of atlases is typically limited
- Changing population characteristics or disease may necessitate new atlases



Segmentation using multi-atlas fusion

Problems:

- Number of atlases is typically limited
- Changing population characteristics or disease may necessitate new atlases

Solutions:

- Can we bootstrap or learn atlases from the population directly?
- Use manifold learning to model characteristics of a population of images

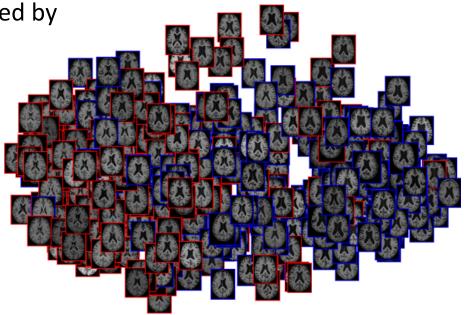
Population modelling

- Space of brain MR images is typically very high-dimensional $(D > 10^6)$
- The natural variation of images may be described in a space with much lower dimension d
- Manifold learning aims at establishing this low-dimensional space
- *N* input images are represented by intensity vectors

$$\mathbf{X} = \{\mathbf{x}_1, ..., \mathbf{x}_N\} \in \mathbb{R}^D$$

• Manifold coordinates are of dimension *d*

$$\mathbf{Y} = \{\mathbf{y}_1, ..., \mathbf{y}_N\} \in \mathbb{R}^d$$



How to measure similarities

• A similarity measure can be defined based on the application:

Shape-based measures

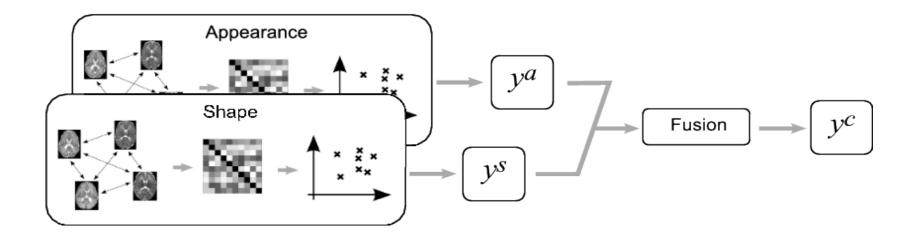
- Distances extracted from the deformation
- Deformation magnitude
- Jacobian determinant
- Other measures extracted from the deformation field

Appearance-based measures

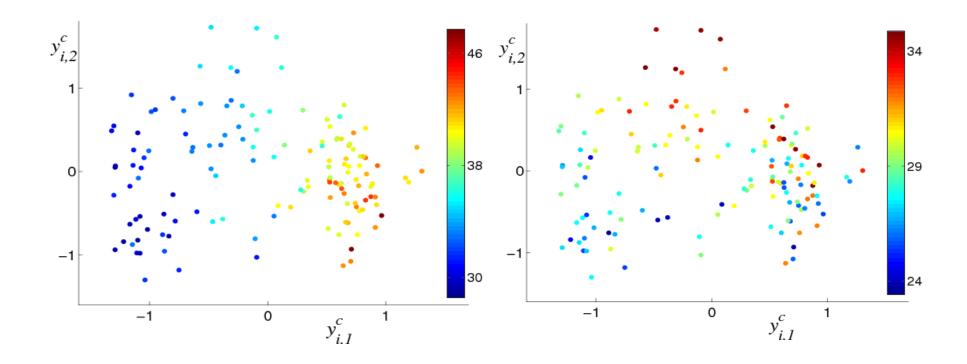
- Similarities extracted from image intensities
- Sums of squared differences (SSD)
- Cross-correlation
- Mutual information
- A weighted measure combining shape and appearance captures both aspects
- Similarities S_{ij} can be transformed to distances D_{ij} and viceversa

How to measure similarities

- Application to neonatal data
- Multiple tailored measures
 - Shape and MR appearance

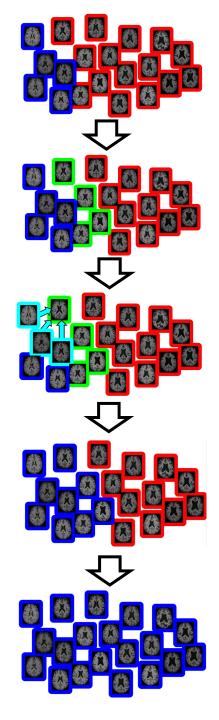


Linking to infant data



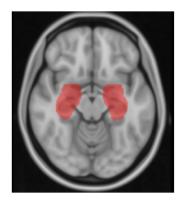
LEAP

- LEAP aims at segmenting diverse image datasets by Learning Embeddings for Atlas Propagation
- Learns new representation for all images
- Neighbourhoods are defined by image similarities
- Initial small set of atlases is propagated throughout the data
- Atlases are propagated to 'nearby' images
- Labelled images are used as *bootstrapped* atlases thereafter

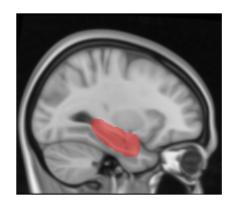


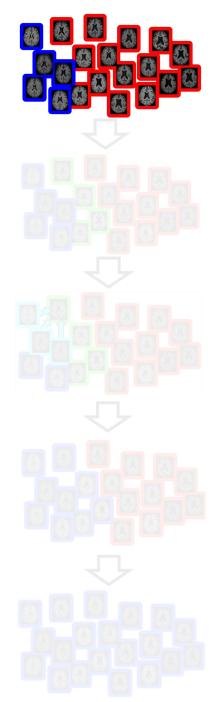
Intensity-based similarities

- Here, we use intensity differences estimated in a template space
- All N images are registered to the MNI152template
- The level of registration can be adapted to the size of the structure of interest
- Pair-wise similarities can be estimated over the whole brain or in a region of interest



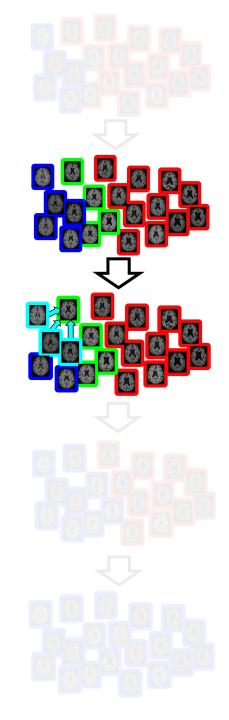






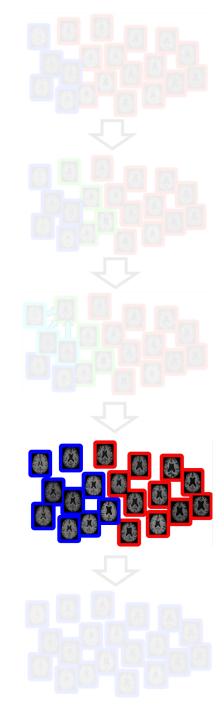
LEAP propagation

- Distances in the learned manifold are used to identify atlas propagation steps
- The *N* unlabelled images that are closest to the set of labelled images are selected for segmentation
- For each selected images, the *M* closest labelled images are selected as atlases
- All selected atlas images are accurately registered to a target image



LEAP propagation (2)

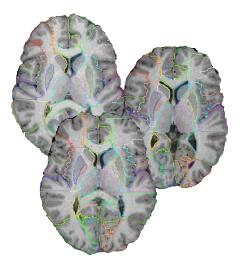
- A spatial prior is generated from multiple atlases
- An intensity model is estimated from the target image
- The target segmentation is estimated based on both models



Application to the segmentation of ADNI

Available set of atlases:

- 30 atlases from young, healthy subjects
- Manually delineated into 83 structures of interest

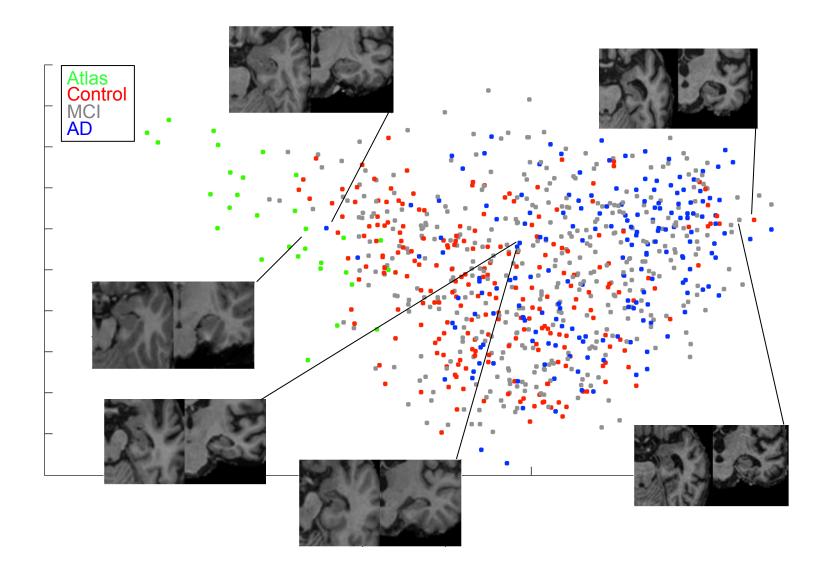


ADNI dataset:

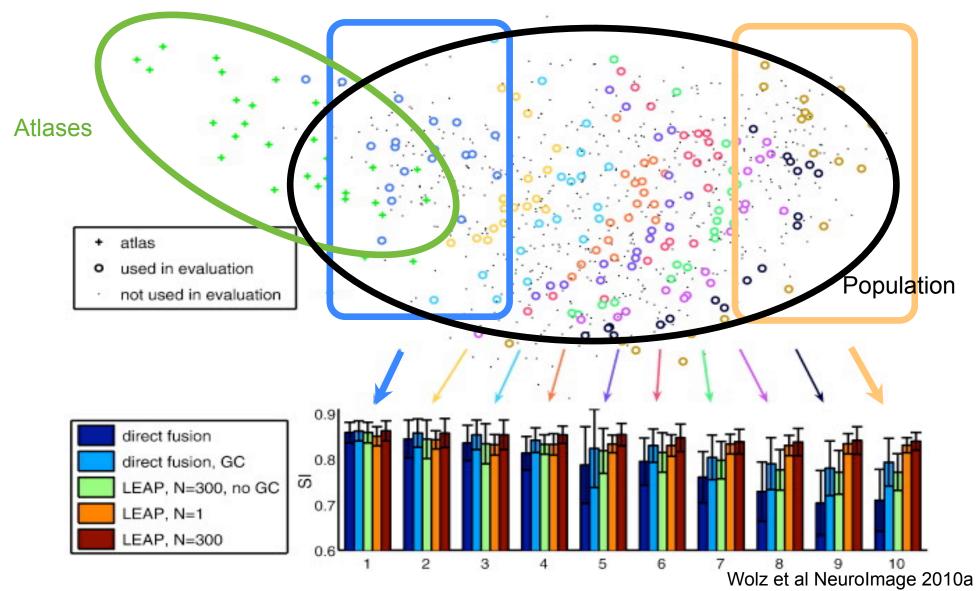
- 838 images from elderly subjects with dementia and age-matched healthy controls
- Strong pathology due to ageing and disease progression



Hippocampal segmentation

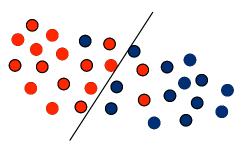


Manifold learning for multi-atlas segmentation: Results



Manifold Learning: classification

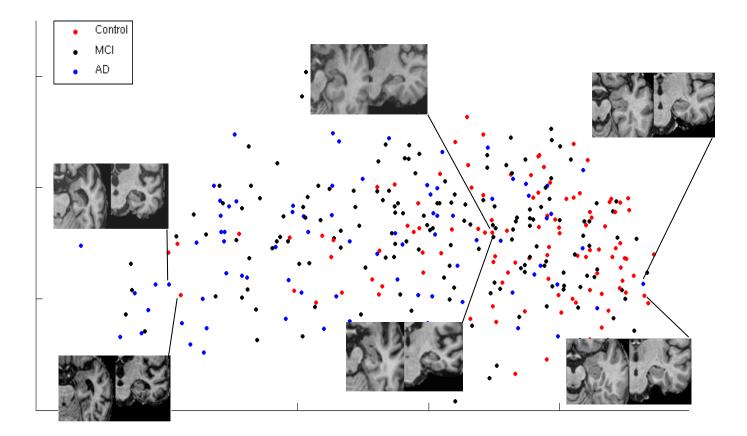
- Manifold coordinates can be directly used to extract information
- Assuming, a clinical label is available for a subset of images, manifold coordinates can be used to classify the unlabelled subjects



2D-embedding

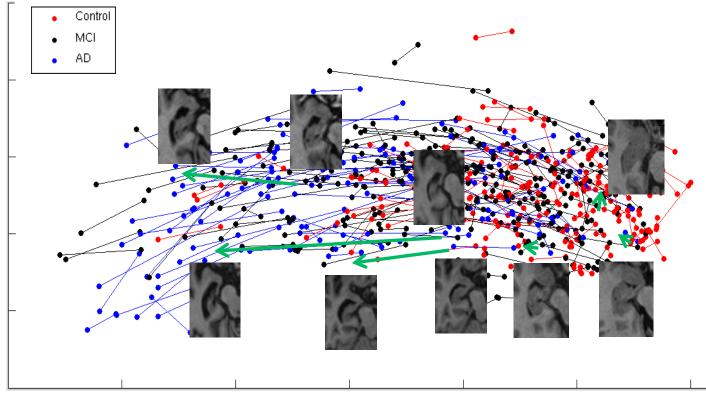
Embedding of baseline images

- 2D embedding of baseline images
- principal axis resembles disease progression



Combined embedding

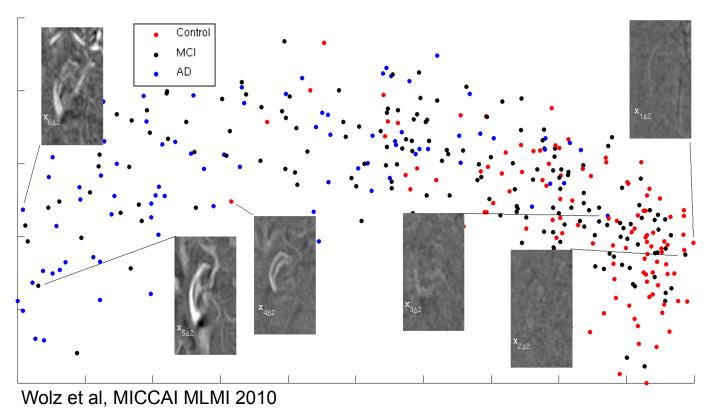
- Single manifold is learned from subjects at two timepoints
- Subjects "move" along principal axis
- More atrophied subjects move "faster"



Wolz et al, MICCAI MLMI 2010

Embedding of intra-subject variation

- Image similarities are based on difference images between baseline and follow-up scans
- Features can be combined with embedding of baseline scans



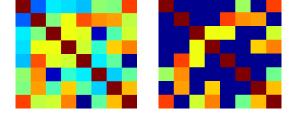
Laplacian Eigenmaps

- All images are represented in a k-nn graph
- Every subject is connected to it's n closest neighbours
- Edge weights w_{ij} are defined by image similarities and form a weight matrix W
- Subjects that are similar in input space are close in manifold space with the objective function

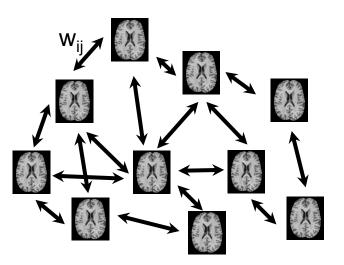
$$\sum_{ij} \left(\mathbf{y}_i - \mathbf{y}_j \right)^2 w_{ij}$$

 Defining the graph Laplacian from the weight matrix W allows a closed form solution [1]

[1] Belkin and Niyogi, 2003, Neur. Comp.



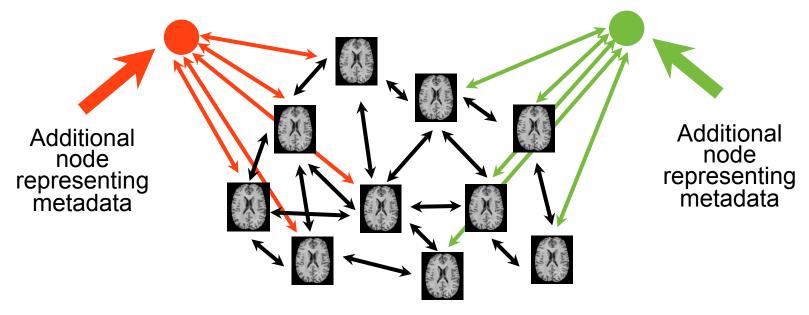
Full similarity matrix k-nn similarity matrix



k-nn neighbourhood graph

Extended similarity graph

- Laplacian eigenmaps only considers image similarities
- Subject metadata (e.g. age, genotype) gives additional information to compare subjects
- An extension of the similarity graph by additional nodes allows to consider such information

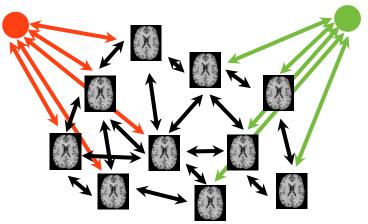


Extended objective function

- In the extended similarity graph, *M* additional nodes represent *M* groups of metadata
- Weights \hat{w}_{im} can be defined discrete or continuously
- An extended objective function can be defined

$$\gamma \sum_{ij} \left(\mathbf{y}_i - \mathbf{y}_j \right)^2 w_{ij} + \sum_{im} \left(\mathbf{y}_i - \mathbf{\hat{y}}_m \right)^2 \hat{w}_{im}$$

- Subjects with similar metadata values are clustered in embedding space
- γ defines the influence of metadata on the final embedding



Illustrative example

- Every node has some meta-information with a value between 0 and 1
- Three additional nodes are introduced in the similarity graph and weights to every image are defined by the metadata
- Changing the influence of the meta-information leads to different embedding results

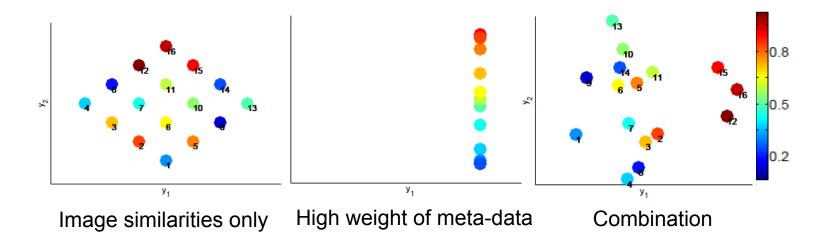


Image data and meta-information

- ADNI baseline images were used for evaluation of the method
- Used non-imaging metadata:
 - CSF concentration of beta amyloid Aβ-42 (continuous)
 - APOE-genotype (discrete)
- Derived imaging metadata:
 - Hippocampal volume (continuous)
- The 420 subjects for which the CSF biomarker was available were used:

	N (F)	MMSE	Αβ-42	ε2/ε4 carriers	Hippo. Vol.
CN	116 (56)	29.1+/-1.0	202+/-58	16/28	4.53+/-0.55
S-MCI	112 (36)	27.2+/-1.8	179+/-62	9/49	4.26+/-0.59
P-MCI	89 (33)	26.6+/-1.8	146+/-46	1/52	3.93+/-0.65
AD	83 (44)	23.6+/-1.9	148+/-46	4/63	3.92+/-0.73

Composite similarity measure

 Pairwise image similarities are based on a combined similarity measure incorporating deformation energy and intensity differences

$$\mathcal{D}_{ij} = \alpha \mathcal{D}_{ij}^{\text{def}} \left(I_i, I_j, \phi_{ij} \right) + \left(1 - \alpha \right) \mathcal{D}_{ij}^{\text{int}} \left(I_i, I_j, \phi_{ij} \right)$$

• Deformation energy is based on the deformation magnitude resulting from registering two images

$$\mathcal{D}_{ij}^{\text{def}}\left(I_i, I_j, \phi_{ij}\right) = \sum_{x \in \Omega} \|u_{ij}(x)\|_2^2 dx$$

• Sums of squared intensity differences are used to represent the residual difference

$$\mathcal{D}_{ij}^{\text{int}}\left(I_{i}, I_{j}, \phi_{ij}\right) = \sum_{x \in \Omega} \left(I_{i}\left(x\right) - I_{j}\left(\phi_{ij}\left(x\right)\right)\right)^{2}$$

Parameter setting

- Classification results on a training data set show a good performance of the similarity-based measure
- Using a 5-10 • 0.78 dimensional 0.76 manifold leads to classificatio accuracy stable classification results 0.7 0.68 0.5 0 0.375 5 10 0.25 α 15 0.125 d 20 25 0

Classification results

- Manifold coordinates are corrected for age
- 1,000 leave-25%-out runs are performed to obtain classification rates

	AD vs CN	P-MCI vs S-MCI	P-MCI vs CN			
Laplacian Eigenmaps	86%	63%	82%			
& ApoE	83%	69%	81%			
& Aβ-42	87%	68%	84%			
& Hippo. Vol.	86%	66%	83%			
& Aβ-42 / Hippo. Vol.	88%	67%	87%			
& Aβ-42 / Hippo. Vol. / ApoE	88%	69%	87%			
Classification assures y using manifold learning						

Classification accuracy using manifold learning

Conclusions

- Manifold learning allows to model the characteristics of a large population of brain images
- In LEAP, the defined metric space is used to propagate a set of manually labelled atlas images in several steps through the whole manifold
- An improved segmentation and classification accuracy shows the benefit of the manifold-based approach
- Manifold coordinates can be directly used to infer from subjects with a clinical label to unlabelled subjects
- An approach to incorporate metadata into Laplacian eigenmaps was described